

Tomographic Terahertz Imaging Using Sequential Subspace Optimization

Thomas Schuster, Anne Wald

Department of Mathematics
Saarland University Saarbrücken

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Introduction

Sequential subspace optimization (SESOP)

- Iterative reconstruction technique for inverse problems
- here: SESOP for nonlinear inverse problems in Hilbert spaces
- Extension (acceleration) of Landweber's method
- Regularization technique (RESESOP)
- reduction of the number of iterations

Terahertz tomography

- novel imaging technique in nondestructive testing for plastics and ceramics
- approach via scattering problems: nonlinear inverse problem
- solution of the inverse problem of THz tomography with an adapted RESESOP method

Introduction

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Notation and definitions

Let X, Y be Hilbert spaces and $M_{F(x)=y} := \{x \in X : F(x) = y\}$ the **solution set** for a nonlinear operator $F : \mathcal{D}(F) \subseteq X \rightarrow Y$.

We assume to have noisy data y^δ with **noise level** $\delta \geq \|y - y^\delta\|$.

Hyperplanes, halfspaces and stripes

Let $u \in X \setminus \{0\}$ and $\alpha, \xi \in \mathbb{R}$, $\xi \geq 0$. We define the (affine) **hyperplane**

$$H(u, \alpha) := \{x \in X : \langle u, x \rangle = \alpha\},$$

the **halfspace**

$$H_{\leq}(u, \alpha) := \{x \in X : \langle u, x \rangle \leq \alpha\}$$

and the **stripe**

$$H(u, \alpha, \xi) := \{x \in X : |\langle u, x \rangle - \alpha| \leq \xi\}.$$

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SESOP iteration for linear problems $Ax = y$ in Hilbert spaces

$$x_{n+1} := x_n - \sum_{i \in I_n} t_{n,i} A^* w_{n,i},$$

I_n a finite index set, $w_{n,i} \in Y$ for all $i \in I_n$, and the parameters $t_n = (t_{n,i})_{i \in I_n}$ minimize

$$h_n(t) := \frac{1}{2} \left\| x_n - \sum_{i \in I_n} t_i A^* w_{n,i} \right\|^2 + \sum_{i \in I_n} t_i \langle w_{n,i}, y \rangle.$$

Lemma [Schöpfer, S., Louis (2008)]

The minimization of $h_n(t)$ is equivalent to computing the metric projection

$$x_{n+1} = P_{H_n}(x_n), \quad H_n := \bigcap_{i \in I_n} H_{n,i},$$

onto the intersection of hyperplanes

$$H_{n,i} := \{x \in X : \langle A^* w_{n,i}, x \rangle = \langle w_{n,i}, y \rangle\} \supseteq M_{Ax=y}.$$

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RESESOP for linear operators and noisy data

Project sequentially onto **intersections of stripes** $H(u, \alpha, \xi)$, where

$$\xi = \xi(\delta), \quad M_{Ax=y} \subseteq H(u, \alpha, \xi).$$

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SESOP for nonlinear inverse problems $F(x) = y$

We consider nonlinear inverse problems

$$F(x) = y, \quad F : \mathcal{D}(F) \subseteq X \rightarrow Y.$$

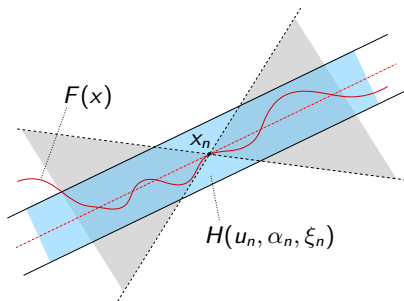
Assume that F satisfies the tangential cone condition

$$\|F(x) - F(\tilde{x}) - F'(x)(x - \tilde{x})\| \leq c_{tc} \|F(x) - F(\tilde{x})\|$$

for $x, \tilde{x} \in B_\rho(x_0)$ and $0 < c_{tc} < 1$. Furthermore,

$$\sup_{x \in B_\rho(x_0)} \|F'(x)\| \leq c_F.$$

- Use stripes also in case of exact data y .
- Take into account the local character as well as the nonlinearity of operators.



From SESOP for linear problems to SESOP for nonlinear problems

Stripes in the linear case

$$H_{n,i}^\delta := \left\{ x \in X : \left| \langle A^* w_{n,i}^\delta, x \rangle - \langle w_{n,i}^\delta, y^\delta \rangle \right| \leq \delta \|w_{n,i}^\delta\| \right\}$$

Stripes in the nonlinear case

$$\begin{aligned} H_{n,i}^\delta := \left\{ x \in X : \left| \langle F'(x_i^\delta)^* w_{n,i}^\delta, x_i^\delta - x \rangle - \langle w_{n,i}^\delta, F(x_i^\delta) - y^\delta \rangle \right| \right. \\ \left. \leq \|w_{n,i}^\delta\| \left(c_{tc} (\|R_i^\delta\| + \delta) + \delta \right) \right\} \supseteq M_{F(x)=y} \end{aligned}$$

RESESOP algorithm

As long as the residual $R_n^\delta := F(x_n^\delta) - y^\delta$ fulfills $\|R_n^\delta\| > \tau\delta$, compute

$$x_{n+1}^\delta = x_n^\delta - \sum_{i \in I_n^\delta} t_{n,i}^\delta F'(x_i^\delta)^* w_{n,i}^\delta \in \bigcap_{i \in I_n^\delta} H(u_{n,i}^\delta, \alpha_{n,i}^\delta, \xi_{n,i}^\delta)$$

and $\|z - x_{n+1}^\delta\|^2 \leq \|z - x_n^\delta\|^2 - C(\|R_n^\delta\|, \delta, c_{tc}, c_F)$ for $z \in M_{F(x)=y}$.

Convergence of the SESOP algorithm

Let

- $n \in I_n$ for each $n \in \mathbb{N}$,
- $I_n \subseteq \{n - N + 1, \dots, n\} \cap \mathbb{N}$, $N \geq 1$ fixed
- $w_{n,i} := R_i = F(x_i) - y$ for each $i \in I_n$,
- $x^+ \in B_{\rho/2}(x_0)$ be the unique solution in $B_\rho(x_0)$.

Theorem

[Wald, S. (2016)]

The sequence of iterates $\{x_n\}_{n \in \mathbb{N}}$, generated by the SESOP algorithm, converges strongly to x^+ , if the optimization parameters $t_{n,i}$ are bounded,

$$|t_{n,i}| \leq t$$

for some $t > 0$ for all $i \in I_n$ and $n \in \mathbb{N}$.

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Convergence and regularization of the RESESOP algorithm

Theorem

[Wald, S. (2016)]

- The RESESOP algorithm, together with the discrepancy principle, where the tolerance parameter satisfies

$$\tau > \frac{1 + c_{tc}}{1 - c_{tc}} > 1,$$

yields a **finite stopping index** $n_*(\delta)$.

- The iterates x_n^δ depend, for a fixed $n \in \mathbb{N}$, continuously on the data y^δ and we have

$$x_n^\delta \rightarrow x_n \quad \text{for } \delta \rightarrow 0.$$

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- The algorithm yields a **regularized solution** $x_{n_*(\delta)}^\delta$ of the nonlinear problem $F(x) = y$, if noisy data y^δ are given, i.e.,

$$x_{n_*(\delta)}^\delta \rightarrow x^+ \quad \text{for } \delta \rightarrow 0,$$

if there is only one solution $x^+ \in B_\rho(x_0)$ and if $\lim_{\delta \rightarrow 0} |t_{n,i}^\delta| < t$ holds for all $n \in \mathbb{N}$ and $i \in I_n^\delta$ for some $t > 0$.

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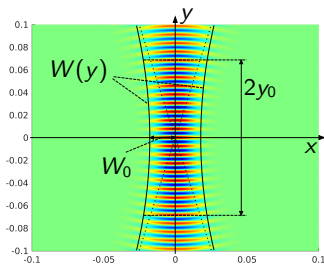
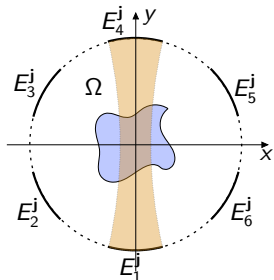
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THz tomography - an introduction

- novel imaging technique in **nondestructive testing** (plastics, ceramics)
- non-ionizing electromagnetic radiation, frequency range **0.1 - 10 THz**
- THz radiation: Gaussian beams with wave number $k_0 = 2\pi f/c$

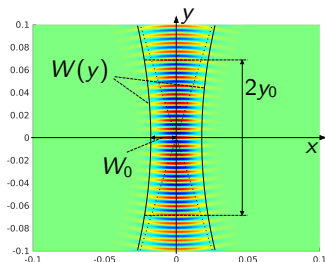
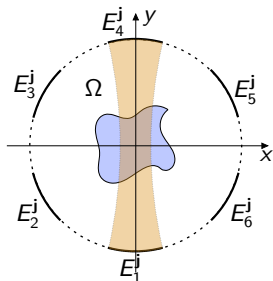


Inverse problem of THz tomography

Reconstruct the complex refractive index $\tilde{n} = n + i\kappa$ to detect defects, inclusions or the moisture content from measurements of the resulting electric field.

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Scattering of THz radiation

For convenience, define

$$m : L^\infty(\Omega) \cap L^2_{\text{comp}}(\Omega) \rightarrow \mathbb{C}, \quad m(\mathbf{x}) := 1 - \tilde{n}^2(\mathbf{x}).$$

By $\Omega \subseteq \mathbb{R}^2$, we denote the domain (with C^1 -boundary $\partial\Omega$) in which m is to be reconstructed.

Boundary value problem for u_t

Given the incident field u_i and m , the total field u_t is determined by

$$\begin{aligned} \Delta u_{\text{sc}} + k_0^2(1 - m)u_{\text{sc}} &= k_0^2 m u_i \quad \text{in } \Omega, \\ \frac{\partial u_{\text{sc}}}{\partial \mathbf{n}} - ik_0 u_{\text{sc}} &= 0 \quad \text{on } \partial\Omega, \\ u_{\text{sc}} + u_i &= u_t \quad \text{in } \bar{\Omega}, \end{aligned}$$

where \mathbf{n} is the outward normal vector of $\partial\Omega$.

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where \mathbf{n} is the outward normal vector of $\partial\Omega$.

Existence and uniqueness of a weak solution

For $m \in L^\infty(\Omega)$ with $\text{Im}(m) \leq 0$, consider the **boundary value problem**

$$\begin{aligned} \Delta u + k_0^2(1 - m)u &= k_0^2 m u_i \quad \text{in } \Omega, \\ \frac{\partial u}{\partial \mathbf{n}} - ik_0 u &= 0 \quad \text{on } \partial\Omega \end{aligned} \tag{BVP}$$

and its **variational formulation**

$$(\nabla u, \nabla v)_{L^2(\Omega)} - k_0^2 ((1 - m)u, v)_{L^2(\Omega)} - ik_0 (u, v)_{L^2(\partial\Omega)} = -k_0^2 (m u_i, v)_{L^2(\Omega)}.$$

Theorem

[Wald, S. (2017)]

The boundary value problem (BVP) possesses a unique weak solution $u \in H^1(\Omega)$, which satisfies

$$\|u\|_{H^1(\Omega)} \leq C_1 \|m\|_{L^\infty(\Omega)} \|u_i\|_{L^2(\Omega)}$$

for a constant $C_1 > 0$.

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The scattering operator S

Definition of S

Let $u_i \in H^1(\Omega)$ and let

$$S : \mathcal{D}(S) \rightarrow H^1(\Omega), \quad m \mapsto u_t = u_i + u_{sc},$$

where

$$\mathcal{D}(S) \subseteq \left\{ m \in L^\infty(\Omega) \cap L^2_{\text{comp}}(\Omega) : \|m\|_{L^\infty(\Omega)} \leq M, \text{Im}(m) \leq 0 \right\}$$

for a fixed $M > 0$ and u_{sc} is the weak solution of (BVP).

Lemma (continuity of S)

[Wald, S. (2017)]

The operator S is well-defined and Lipschitz-continuous on $\mathcal{D}(S)$, more precisely

$$\|S(m_1) - S(m_2)\|_{H^1(\Omega)} \leq C_2 \|m_1 - m_2\|_{L^\infty(\Omega)} \|u_i\|_{L^2(\Omega)},$$

where $C_2 = C_2(k_0, \Omega) > 0$.

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Properties of the scattering operator S

Theorem (Fréchet differentiability)

[Wald, S. (2017)]

The operator S is Fréchet differentiable w.r.t. $m \in \mathcal{D}(S)$ with continuous Fréchet derivative

$$S'(m) : \mathcal{D}(S) \rightarrow H^1(\Omega), \quad h \mapsto S'(m)h = w,$$

where $w \in H^1(\Omega)$ solves the boundary value problem

$$\begin{aligned} \Delta w + k_0^2(1 - m)w &= k_0^2 S(m) \cdot h \quad \text{in } \Omega, \\ \frac{\partial w}{\partial \mathbf{n}} - ik_0 w &= 0 \quad \text{on } \partial\Omega. \end{aligned}$$

Lemma (tangential cone condition)

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For $m_1, m_2 \in \mathcal{D}(S)$, the operator S fulfills the estimate

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The forward operator F

Tomographic measurements

The tomograph (emitter and receivers) are rotated on a circle around the object m , i.e.,

the incident field u_i^j depends on the position $j \in \{1, \dots, J\}$ of the tomograph.

The same holds for the scattered and total field and the scattering map S^j .

The (nonlinear) forward operator F^j

Let

$$F = (F^1, \dots, F^J) : \mathcal{D}(S) \rightarrow \mathbb{C}^{N \times J},$$

where $F^j(m) := Q^j \gamma S^j(m)$ and

$$\gamma : H^1(\Omega) \rightarrow L^2(\partial\Omega), \quad u \mapsto u|_{\partial\Omega}$$

denotes the *trace operator* and the linear operator $Q^j : L^2(\partial\Omega) \rightarrow \mathbb{C}^N$,

$$y_\nu^j = (Q^j v)_\nu = \int_{\partial\Omega} \chi_{E_\nu^j}(\mathbf{x}) v(\mathbf{x}) \, ds_{\mathbf{x}}, \quad \nu = 1, \dots, N$$

describes the *measuring process*.

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Evaluation of the gradient g

The inverse problem of 2D THz tomography

Reconstruct $m : \Omega \rightarrow \mathbb{C}$ from measurements $y^{j,\delta} \in \mathbb{C}^N$ of the electric field, where

$$F^j(m) = y^j, \quad \|y^{j,\delta} - y^j\| \leq \delta, \quad j = 1, \dots, J.$$

(RE)SESOP and Landweber method

We use the gradient

$$g^j(m) := ((F^j)'(m))^* (F^j(m) - y^{\delta})$$

of the functional

$$\Psi^j(m) := \frac{1}{2} \|F^j(m) - y^{\delta}\|^2$$

as search directions.

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The linearity of γ and Q^j yields

- $(F^j)'(m) = Q^j \gamma (S^j)'(m)$,
- $(F^j)'(m)^* = (\gamma (S^j)'(m))^* (Q^j)^*$.

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of the functional

$$\Psi^j(m) := \frac{1}{2} \|F^j(m) - y^\delta\|^2$$

as search directions.

The linearity of γ and Q^j yields

- $(F^j)'(m) = Q^j \gamma (S^j)'(m)$,
- $(F^j)'(m)^* = (\gamma (S^j)'(m))^* (Q^j)^*$.

Adjoint operators

Theorem

[Wald, S. (2017)]

For $R \in L^2(\partial\Omega)^*$ there exists a $\phi \in H^1(\Omega)$ such that

$$(\gamma S'(m))^* R = -k_0^2 \overline{S(m)} \phi$$

holds, where

$$\begin{aligned} \Delta\phi + k_0^2(1 - \bar{m})\phi &= 0 \quad \text{in } \Omega, \\ \frac{\partial\phi}{\partial\mathbf{n}} + ik_0\phi &= -R \quad \text{on } \partial\Omega. \end{aligned}$$

For $\beta = (\beta_\nu)_{\nu=1,\dots,N} \in \mathbb{C}^N$, we thus have

$$((F^j)'(m))^* \beta = (\gamma(S^j)'(m))^* (Q^j)^* \beta = -k_0^2 \overline{S^j(m)} \phi,$$

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Numerical experiments - some adjustments

Landweber method

$$m_{n+1}^\delta = m_n^\delta - \omega F'(m_n^\delta)^* (F(m_n^\delta) - y^\delta) = m_n^\delta - \omega g_n^\delta$$

Two adaptations

- (1) Use **averaged gradients**

$$g_n^\delta := \frac{1}{J} \sum_{j=1}^J g_n^{j,\delta} = \frac{1}{J} \sum_{j=1}^J \left((F^j)'(m_n^\delta) \right)^* \left(F^j(m_n^\delta) - y^{j,\delta} \right).$$

- (2) Adapt (RE)SESOP method to solve nonlinear inverse problems in **complex** Hilbert spaces.

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RESESOP iteration for complex-valued problems

$$m_{n+1}^{\delta} = \left(\operatorname{Re}(m_n^{\delta}) - \sum_{l \in I_n^{\delta}} t_{n,l}^{\delta,r} \cdot \operatorname{Re}(g_l^{\delta}) \right) + i \cdot \left(\operatorname{Im}(m_n^{\delta}) - \sum_{l \in I_n^{\delta}} t_{n,l}^{\delta,i} \cdot \operatorname{Im}(g_l^{\delta}) \right)$$

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RESESOP iteration for complex-valued problems

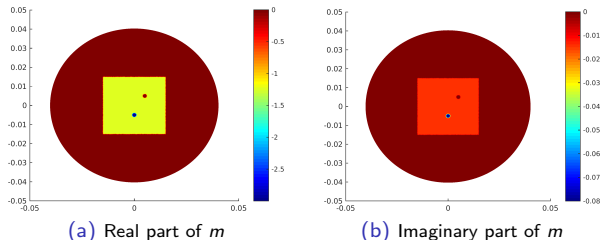
$$m_{n+1}^{\delta} = \left(\operatorname{Re}(m_n^{\delta}) - \sum_{l \in I_n^{\delta}} t_{n,l}^{\delta,r} \cdot \operatorname{Re}(g_l^{\delta}) \right) + i \cdot \left(\operatorname{Im}(m_n^{\delta}) - \sum_{l \in I_n^{\delta}} t_{n,l}^{\delta,i} \cdot \operatorname{Im}(g_l^{\delta}) \right)$$

An example in the Terahertz regime

Three different complex refractive indices:

$$m_1 = -1.249975 - i \cdot 0.015, \quad m_2 = 0, \quad m_3 = -2.2396 - i \cdot 0.072$$

Algorithm: RESESOP with two search directions, $I_n^\delta = \{n - 1, n\}$

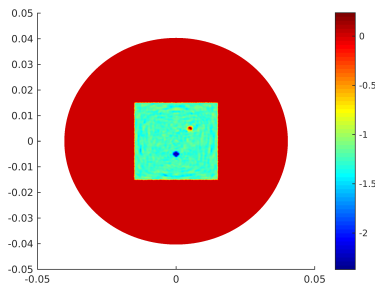


Parameters of the experiment

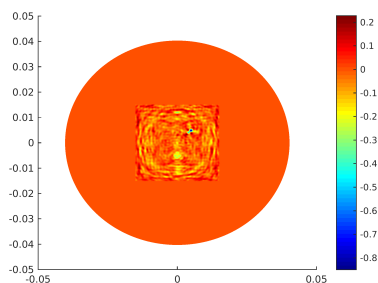
$$f = 0.1 \text{ THz}, \quad N = 40, \quad J = 180, \quad c_{tc} = 0.9, \quad \tau = 20$$

An example in the Terahertz regime

- Assumption: The outer interfaces of the object are known.
- Noise level δ : 2% noise plus error from implementation



(a) Reconstruction of $\text{Re}(m)$

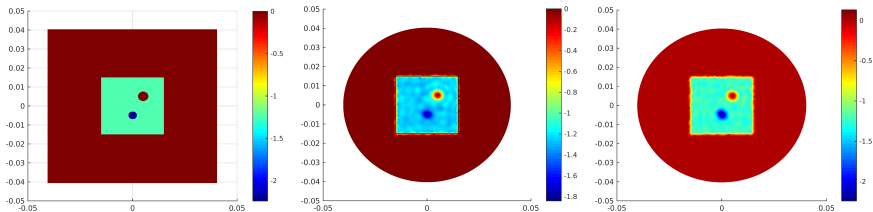
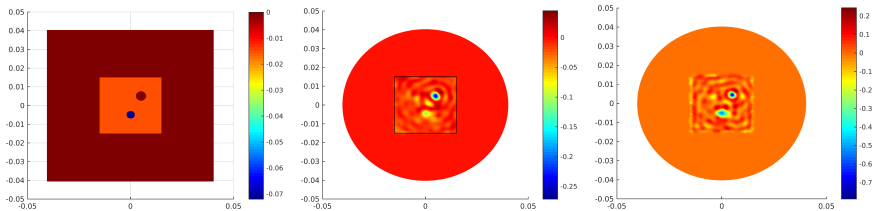


(b) Reconstruction of $\text{Im}(m)$

- Relative error in reconstruction of $\text{Re}(m)$: 7.98 %
- Relative error in reconstruction of $\text{Im}(m)$: > 100 %
- $n_* = 30$ iterations in 14h 13min 51s

A comparison of Landweber and RESESOP method for $f = 2.5 \cdot 10^{10}$ Hz

Landweber: 155 iterations in 5h 38min 49s, **RESESOP:** 20 iterations in 1h 12min 40s

(a) $\text{Re}(m)$ (b) Landweber: $\text{Re}(m_{n_*}^\delta)$ (c) RESESOP: $\text{Re}(m_{n_*}^\delta)$ (d) $\text{Im}(m)$ (e) Landweber: $\text{Im}(m_{n_*}^\delta)$ (f) RESESOP: $\text{Im}(m_{n_*}^\delta)$

Conclusion and outlook

Summary of the results

- extension of SESOP and RESESOP techniques to nonlinear inverse problems in Hilbert spaces
- proof of convergence and regularization results
- modeling and analysis of the inverse problem of THz tomography
- application of SESOP techniques in parameter identification significantly reduces computation time

Future research

- extension of subspace optimization techniques to nonlinear inverse problems in Banach spaces
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Thank you for your attention!